

# Formulation and Development of Tara Gum-mediated Tablets for Delivery of Anticancer Drugs

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#### Abstract

**Background:** Natural polysaccharide tara gum (TG) has been investigated for several biological uses. The current study involved the administration of imatinib, an anticancer model medication, via TG.

**Methods:** Imatinib-modified release tablets were developed using a direct compression method with different concentrations of TG and other excipients. Compressed tablets were evaluated for physicochemical properties.

**Result:** All formulations had an *in vitro* disintegration time ranging from 10–23 min. Among the formulations, F6 exhibited excellent extended-release behaviour with 72% release over 12 h. TG tablets were rich in phytoconstituents, including saponins, tannins, phenolics, flavonoids, carbohydrates, proteins, and amino acids.

**Conclusion:** TG has potential in the drug delivery application of anticancer medications as a rate-retarding polymer.

#### Keywords

Imatinib, modified release, natural gums, phytochemicals, tara gum.

# Introduction

Natural polymers are increasingly favored in the pharmaceutical industry for drug delivery systems due to biocompatibility, biodegradability, and capacity for chemical modification. These materials, including chitosan, alginate, and hyaluronic acid, can be tailored to create drug delivery systems, such as nanoparticles, hydrogels, and micelles [1]. The biocompatible nature of natural polymers reduces the risk of adverse immune reactions, enhancing the safety profile of drug delivery systems [2]. Moreover, the biodegradability of natural polymers ensures degradation into non-toxic byproducts, minimizing the risk of long-term accumulation and associated toxicity [3]. The ability of these polymers to be chemically modified allows for precise control over drug release profiles, which is essential for maintaining therapeutic levels over extended periods, especially in the treatment of chronic conditions [4]. Natural polymers have a critical role in the pharmaceutical industry due to biocompatibility, biodegradability, and ability to be chemically modified. These materials, like chitosan, alginate, and hyaluronic acid, can be tailored to create drug delivery systems, including nanoparticles, hydrogels, and micelles [1]. The biocompatible nature of natural polymers minimizes adverse immune responses and enhances the safety profile of the drug delivery system [2]. The biodegradability of natural polymers ensures break down into non-toxic byproducts, which are easily eliminated from the body, thereby preventing long-term accumulation and associated toxicity [3]. Additionally, the inherent ability of natural polymers to be chemically modified allows drug release profiles to be fine-tuned, ensuring sustained and controlled release of therapeutic agents over extended periods [4]. This feature is particularly advantageous for chronic conditions requiring long-term medication adherence. Excellent mucoadhesive qualities are also exhibited by natural polymers, which increase medication bioavailability by extending the duration of drug residency at the absorption site [5]. Furthermore, structural versatility allows for encapsulation of proteins, peptides, and small molecules, thereby broadening the scope of treatable conditions. Overall, natural polymers are integral to developing advanced <sup>1</sup>Suresh Gyan Vihar University, Jaipur, Rajasthan, India

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drug delivery systems that improve therapeutic efficacy and patient compliance [6].

Tara gum (TG), a natural polysaccharide derived from the seeds of the Caesalpinia spinosa tree, belongs to the galactomannan family. This hydrocolloid is valued for thickening, stabilizing, and gelling properties, which have applications in various industries, including pharmaceuticals [7, 8]. The high molecular weight of TG, which is composed of mannose and galactose units, contributes to exceptional viscosity and gel-forming capabilities, making TG an ideal candidate for rate-retarding applications in drug delivery [9]. The ability of TG to form viscous solutions at low concentrations enhances the bioavailability and therapeutic efficacy of active pharmaceutical ingredients (APIs). Furthermore, the mucoadhesive properties of TG increase the residence time of drugs at the absorption site, which is particularly beneficial for oral and buccal drug delivery systems. The stability of TG across a wide range of pH conditions and compatibility with other polymers and excipients further expand the utility of TG in diverse drug delivery applications [10, 11]. The stability of TG in various pH conditions and compatibility with other polymers and excipients further enhance the application of TG in formulating diverse drug delivery systems. Overall, the natural origin and functional properties of TG make TG a valuable component in modern pharmaceutical formulations [12].

Despite the success of conventional drug delivery systems, there remains significant challenges in the controlled release and bioavailability of anticancer medications. Tyrosine kinase inhibitors (TKIs), such as imatinib, which are widely used in treating gastrointestinal stromal tumors (GISTs) and chronic myeloid leukemia (CML), are limited by rapid drug clearance and the need for frequent dosing and can lead to decreased patient compliance and potential side effects [13]. The potential of TG to overcome these limitations through rate-retarding and mucoadhesive properties makes TG a promising candidate for improving the delivery and efficacy of anticancer medications. However, application of TG in anticancer drug delivery, especially in tablet formulations, remains underexplored. The mechanism of action for TKIs involves blocking the BCR-ABL protein, which promotes cancer cell growth [13]. Imatinib revolutionized CML treatment and significantly improved patient outcomes and survival rates. Natural polysaccharide TG has been investigated for a number of biological uses [14, 15]. In the current study we selected the anticancer agent, imatinib, as a model drug to further explore drug delivery application.

Table 1 Formula Composition of 50-mg Imatinib Tablets

This study aimed to determine the potential of TG as a natural polymer for developing controlled-release tablets of imatinib. By leveraging the unique properties of TG, this study sought to address the challenges of conventional anticancer drug delivery systems, providing a more effective and patient-friendly formulation.

# Materials and methods

## **Materials**

The plant material (TG isolate) and other excipients, such as talc, Aerosil<sup>®</sup>, magnesium stearate, lactose DCL-21, and sodium starch glycolate, were obtained from Vineet Analytical Research Laboratories Pvt Ltd. (Pioma Chemicals, Mumbai, Maharashtra, India).

## Formulation of tablets using TG

Tablets containing imatinib were developed using TG extract. Conventional tablets were made with a variable ratio of excipients to TG utilizing the direct compression process. All excipients were well-mixed except magnesium stearate. Following adequate mixing of the extract and other ingredients, Aerosil<sup>®</sup> and magnesium stearate were added and combined for a further 2–3 min. A rotary punching machine with a 6-mm flat punch was used to crush the tablets [16]. The composition of all formulations is listed in Table 1.

# **Characterization of tablets [17]**

### Thickness

Tablet thickness was measured using vernier caliper and recorded.

### Weight variation

A sample of 20 tablets was obtained at random from each batch and weighed separately. Twenty tablets were weighed and the average and standard deviation were determined. If no tablet weight deviated from the average weight by more than the percentage shown in **Table 1** and no tablet weight

Sr. No	Ingredients	F1	F2	F3	F4	F5	F6
1	Imatininb	50	50	50	50	50	50
2	TG	100	120	140	160	180	200
3	Talc	10	10	10	10	10	10
4	Aerosil®	8	8	8	8	8	8
5	Magnesium stearate	4	4	4	4	4	4
6	Lactose DCL-21	158	128	98	68	38	8
7	Sodium starch glycolate	50	60	70	80	90	100
8	Total	380	380	380	380	380	380

All quantities are in mg.

deviated by more than twice that percentage, the batch passed the weight variation test.

#### Hardness

Hardness was measured using a Pfizer hardness tester (Dolphin Pharmacy, Mumbai, Maharashtra, India).

#### Friability

A Roche friabilator (Testing lab Instruments, Mumbai, Maharashtra, India) was filled with 20 weighted tablets and revolved at 25 rpm for 4 min. The tablets were re-weighed after dedusting and revolutionizing. The friability was calculated using the following equation:

$$\%F = \{1 - (W, /W)\} \times 100$$

where,

%F = % friability W = Initial weight of the tablet W = tablet weight after revolution.

## **Disintegration test**

Six cylindrical glass tubes were supported by a rigid basket rack assembly in which the tablets were placed. The glass tube dimensions were as follows: length,  $77.5\pm2.5$ mm; internal diameter, 21.5 mm; and wall thickness, 2 mm. The assembly was suspended in a 1000-ml beaker in liquid media. The amount of liquid was such that the lowest point of the wire mesh was 25 mm below the liquid surface and 25 mm above the beaker bottom. A temperature of  $37^{\circ}$ C was kept constant. The average disintegration time was noted.

#### Table 2 Physical Properties of Imatinib Tablets

## **Content uniformity**

The drug content of imatinib tablets was determined by weighing 10 tablets from each formulation and grinding the tablets into a fine powder. After dissolving part of the powder in methanol (20 mg of imatinib), the mixture was filtered through filter paper. After an appropriate dilution, the absorbance at 238 nm was measured using a UV-visible spectrophotometer to determine the amount of imatinib present.

## Phytochemical screening

The optimized tablet formulation was used for the initial phytochemical per standard procedures [18].

### In vitro dissolution study

The USP type-II dissolving apparatus was utilized for performing dissolution. A paddle and 1000 ml of 0.1N HCl at  $37\pm0.5$ °C made up the dissolving medium and stirrer running at 50 rpm. One tablet was used in each test. The dissolving liquid was drawn out in increments of 10 ml between 5 and 60 min in advance. An equivalent volume of new media was used to replace the samples that were removed. The samples were subsequently run through a 0.45-µ membrane filter paper and the absorbance at 238 nm was determined. The drug amount was calculated using a calibration curve and recorded as the total quantity of medication dissolved. Three duplicates of the dissolution investigations were completed.

Batch No.	Weight Variation (mg)	Thickness (mm)	Diameter (mm)	Friability (%)	Hardness (N)	DT (min.)	Drug Content (%)
F1	385.2±9.48	8.5±0.2	6.04±0.03	0.8	5.3±0.9	16	98.20±1.12
F2	382.4±1.52	8.4±0.3	6.00±0.13	0.76	4.9±0.4	14	98.21±1.80
F3	381.8±1.62	8.5±0.1	6.02±0.02	0.6	4.0±0.6	18	98.41±1.50
F4	384.2±1.26	8.4±0.2	6.03±0.01	0.86	4.8±0.5	17	98.11±1.13
F5	380.7±1.64	8.4±0.3	6.02±0.01	0.93	4.6±0.3	23	98.56±0.99
F6	383.4±1.38	8.5±0.1	6.03±0.02	0.45	4.7±0.8	10	100.20±1.1

#### Table 3 Comparative Drug Release Profile in 0.1N HCI

Time	% Drug Release From Formulation						
(hr)	F1	F2	F3	F4	F5	F6	
0	0	0	0	0	0	0	
1	25	22	20	18	16	12	
2	40	36	32	29	25	20	
4	50	48	44	40	37	30	
6	65	62	59	55	51	41	
8	78	75	71	69	55	49	
10	90	85	79	71	67	65	
12	99	97	93	89	82	72	



Figure 1 Comparative dissolution profile of imatinib tablets in 0.1N HCl.

# **Results and discussion**

**Brief Report** 

# Development of imatinib tablets containing TG

The extracted TG mucilage was utilized for the development of extended-release tablets with varying concentrations of TG. The tablets were manufactured using a direct compression method. The direct compression technique for tablet formulation is crucial because the direct compression technique simplifies the manufacturing process, reduces production costs, and enhances stability [19]. The direct compression technique eliminates the need for wet granulation, thus avoiding heat and moisture, making the direct compression technique ideal for moisture-sensitive and heat-labile drugs [20]. The developed tablets were characterized for physical parameters, which are presented in **Table 2**.

A round punch (6 mm in diameter) was used to compress the tablets. The diameter of the compressed tablets ranged from  $6.00\pm0.13$  mm to  $6.04\pm0.03$  mm, which is acceptable (acceptance criteria,  $\pm 2\%$  to  $\pm 5\%$  of the punch

diameter [5.70–6.30 mm]) given the punch dimensions. Minimal weight variation was observed, ranging from  $380.7\pm1.64-385.2\pm9.48$  mg (acceptance limit,  $\pm7.5\%$  of the tablet weight) due to the excellent flow properties of the granules that ensured complete die filling. The content uniformity was excellent, ranging from  $100.20\pm1.1-98.11\pm1.13\%$ , meeting the USP limit for uncoated tablets weighing >324 mg, which requires content uniformity within 5%. Tablet hardness ranged from  $4.0\pm0.6-5.3\pm0.9$  N. Friability, assessed using a Roche friabilator, was within the acceptable range of 0.45-0.93% (acceptance criteria, <1%). The thickness of the tablets ranged from  $8.4\pm0.2-8.5\pm0.2$  mm. All formulations had an *in vitro* disintegration time ranging from 10-23 min.

## In vitro dissolution study

The comparative dissolution profile is presented in **Table 3** and **Figure 1**. All formulation batches were shown to have extended release behavior. Among the formulations, F6 exhibited excellent extended release behavior with 72% release over 12 h. **Table 3** shows the percentage drug release with respect to time for all the formulations.

The ability of cancer therapy tablets to exhibit extendedrelease behavior is essential because a steady and sustained release of the medication is guaranteed, preserving therapeutic levels in the circulation for a longer amount of time [21]. By reducing the frequency of dose, patient compliance and convenience are enhanced. Sustained release also helps maintain steady-state drug concentrations, reducing the risk of peaks and troughs that can lead to side effects or sub-therapeutic effects. Controlled release enhances the efficacy of treatment, potentially leading to better outcomes in managing cancer [22]. This approach also targets specific timing for drug release, aligning with circadian rhythms for optimal effectiveness.

Table 4 Phytochemical Test of Different Formulations at Different Time Intervals

Sr. No.	Plant Constituents	Test/Reagent	TG Tablet
1	Steroids	Salkovaski	
2	Alkaloids	Dragendroff's test	
		Hager's test	
		Mayer's test	
		Wagner's test	
3	Saponins	Foam test	++
		Hemolysis test	++
4	Fats and oils	Filter paper test	
5	Tannins and Phenolic	Ferric chloride test	++
		Lead acetate test	++
		Potassium dichromate	++
		Bromine water	++
6	Flavonoids	Shinoda test	++
		Lead acetate test	
7	Carbohydrates	Molisch test	++
		Fehling's test	++
		Barfoed's test	++
8	Proteins	Millon's test	++
		Biuret test	++
9	Amino acid test	Ninhydrin test	++

+ve: present; --ve: absent.

## **Phytochemical screening**

The results of the phytoconstituents are presented below.

Steroids, alkaloids, fats, and oils were absent in TG mucilage tablets. Other important phytoconstituents, such as saponins, tannins, phenolics, flavonoids, carbohydrates, proteins, and amino acids, were abundantly present (**Table 4**). The phytochemical screening revealed that TG is rich in phytoconstituents and might be researched as a potential natural remedy for a range of ailments.

# Conclusion

In the current study, TG was shown to be efficiently used as a rate-retarding natural polymer and successfully explored in drug delivery of anticancer agents. All the table parameters were within an acceptable range with excellent modified release properties for a period of 12 h. Moreover, TG tablets are rich in various phytoconstituents, including saponins, tannins, phenolics, flavonoids, carbohydrates, proteins, and amino acids.

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